



# Effect of denoising on brain atrophy measurements based on MRI for Alzheimer's disease

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Mojmir Vinkler, Stanislav Katina

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Masaryk University

# Dataset from two Phase I studies

## Clinical Trials

**Axon CO 18700** – A 3-months randomized, placebo-controlled, parallel group, double-blinded, multi-centre, phase I study to assess tolerability and safety of AADvac1 applied to patients with mild to moderate Alzheimer’s disease with a 3-months open label extension period.

**AC-AD-002 “FUNDAMANT”** – An 18-months open label phase I follow-up study on patients with Alzheimer’s disease who have completed the AADvac1 phase I study “AXON CO 18700”.

## Key people

Clinical Project Leader: **Prof. Michal Novak** (AXON Neuroscience CRM Services SE, Bratislava, Slovakia)

Senior Medical Analyst: **Petr Novak**, MD (AXON Neuroscience CRM Services SE, Bratislava, Slovakia)

Brain Imaging Analyst: **Miroslav Smisek**, MD (AXON Neuroscience CRM Services SE)

## Principal Investigators

**Univ. Prof. Dr. Reinhold Schmidt** (Medizinische Universität Graz, Graz, Austria)

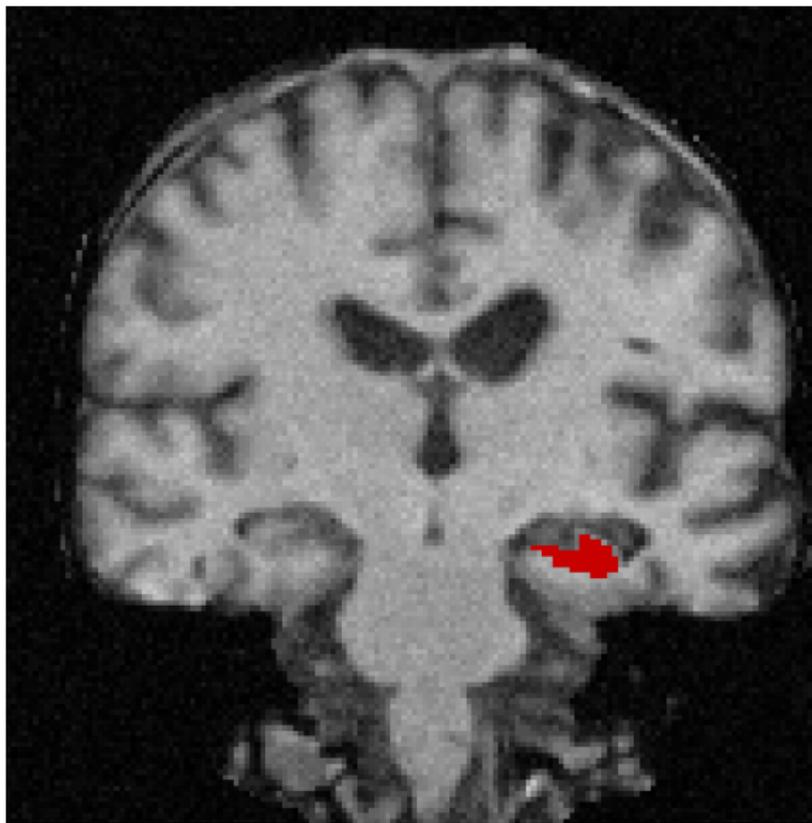
**Univ. Prof. Dr. Peter Dal-Bianco** (Medizinische Universität Wien, Wien, Austria)

**Dr. Susanne Grininger** (Universitätsklinik für Neurologie, Christian-Doppler-Klinik, Salzburg, Austria)

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# The Brain



# Introduction

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# Goals

## Goal I

Reduce variance in volumetric measurements with denoising across multiple scans of single patient.

## Goal II

Measure atrophy of brain and other ROIs (hippocampus) and assert its difference between placebo and verum (treated) groups.

# Dataset Characteristics

	Verum (n=22)	Placebo (n=6)
Age	67.3 ± 6.7 [53-77]	68.5 ± 12.4 [55-82]
Sex, male	10 (45%)	6 (100%)
Scans	5 ± 0	5 <sup>1</sup> ± 0
MRI	1.5T (80%), 3T (20%)	1.5T (100%), 3T (0%)

## Other details

- First phase out of three phases
- 5 MRI scans for each patient within 180 days
- Repeated scans when poor quality scan was observed
- 3 measuring sites, different quality of MRI scans (1.5T, 3T)

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<sup>1</sup>Patients were given vaccination at their third visit

# Denoising

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## Why denoising MRI?

- Registration / segmentation methods are often sensitive to noise in data
- Many available softwares do not use denoising or use less effective methods (such as gaussian smoothing) which can lead to sub-par results

## What's hard about denoising MRI?

- Noise has Rician distribution which is similar to Gaussian in high intensity areas, but non-Gaussian in the background
- Computationally much more demanding than denoising 2D images - a lot of papers deal with optimizing existing methods for 3D

## Gaussian smoothing

## Non-local means

Currently state of the art in terms of performance and visual quality

## Anisotropic diffusion

Image is diffused according to given PDE, similar to gaussian smoothing, but preserves edges

## Fourier / Wavelet based methods

Transform to frequency domain, remove noise there and then transform back

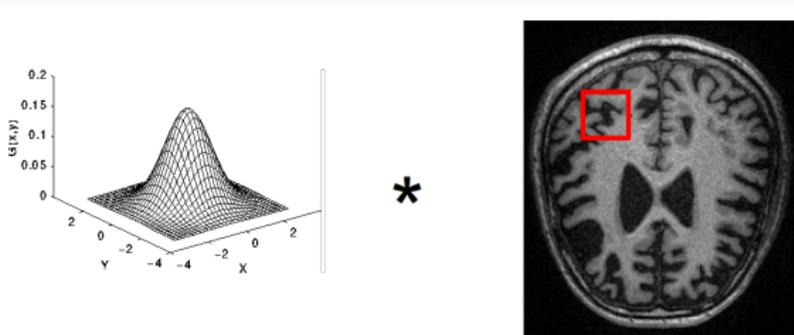
# Gaussian Smoothing

- Convolution with the Gaussian kernel
- “Blurs” the image including edges
- Super-fast computation and super-easy implementation

$$\mathcal{GS}(x) = \frac{\int_{N(x)} w(x, y) u(y) dy}{\int_{N(x)} w(x, y) dy},$$

where  $w(x, y)$  is a standard Gaussian kernel

$$w(x, y) = \frac{1}{\sqrt{2\pi}h^2} e^{-\frac{|x-y|^2}{2h^2}}.$$



# Non-local Means

Let  $u : \Omega \rightarrow \mathbb{R}$  represent image intensity, then

$$\mathcal{NL}(x) = \frac{\int_{\Omega} w(x,y)u(y)dy}{\int_{\Omega} w(x,y)dy},$$

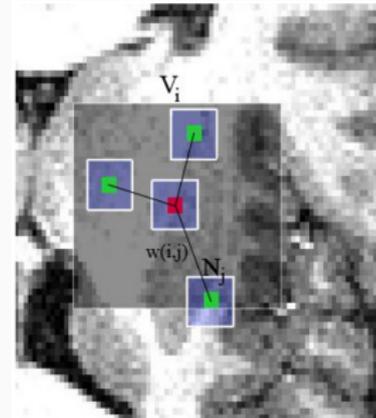
where

$$w(x,y) = e^{-\frac{|N(x)-N(y)|^2}{h^2}}$$

with  $N$  being a neighborhood and  $h$  acting as a smoothing parameter.

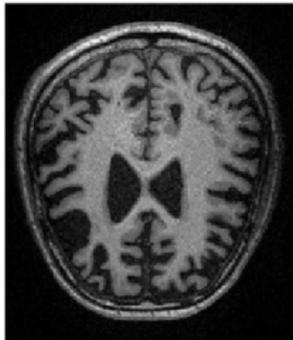
*= Find the most similar neighborhoods to neighborhood of a processed voxel and average their intensities.*

Needs some optimizations to finish computation in a reasonable time



# Methods side-by-side

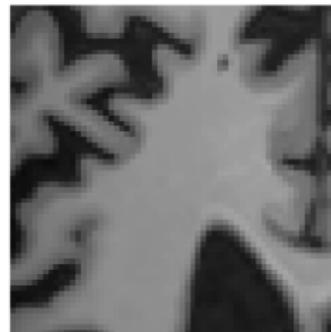
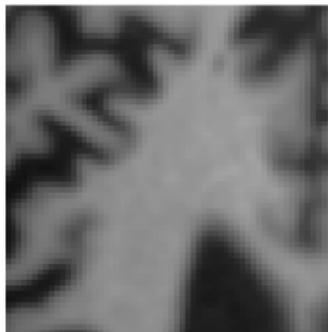
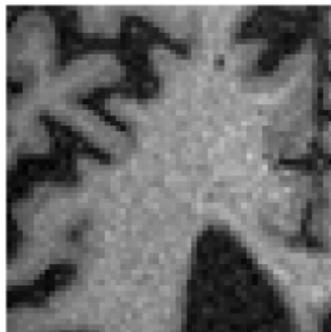
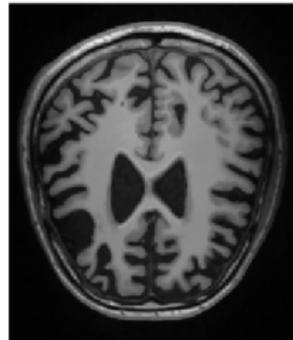
Raw



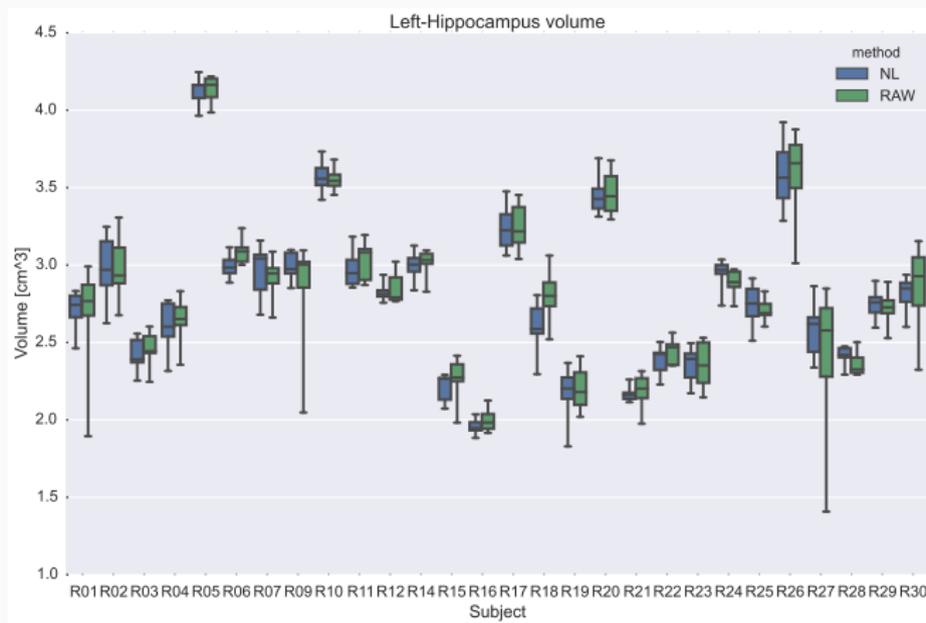
Gaussian Smoothing



Non-local Means



# Effect of Smoothing on Volume Measurements



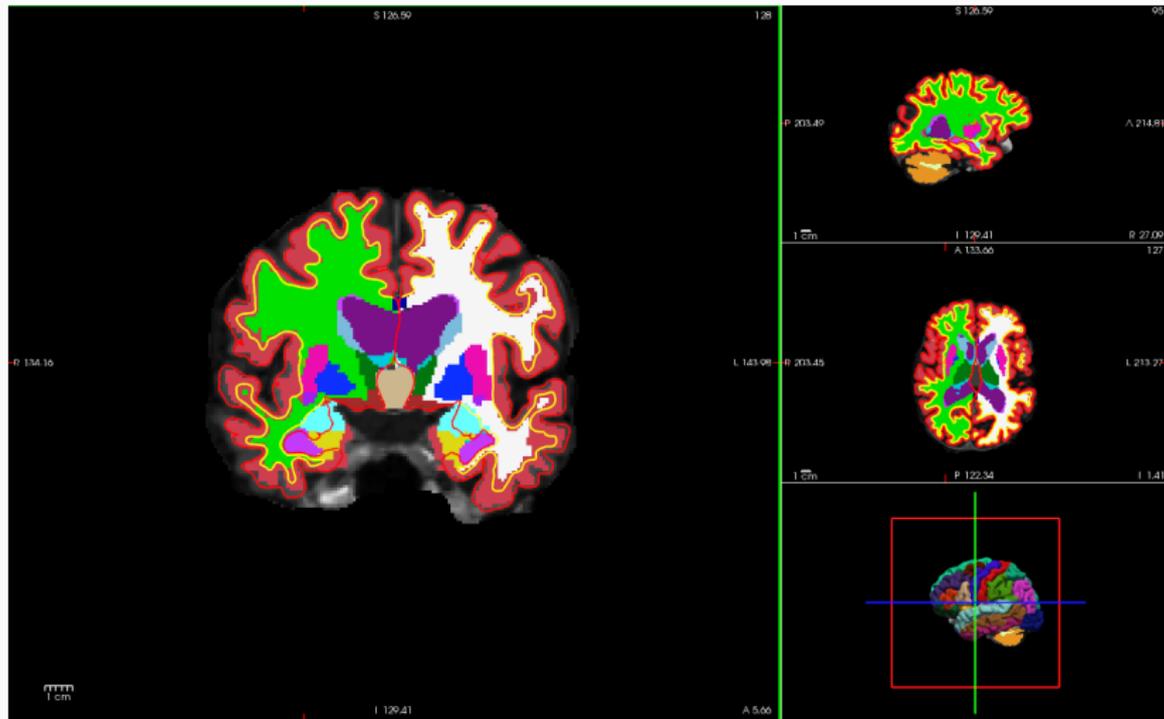
Error reduction from 6.79% to 3.54%

Detailed view <https://multi-armed-bandit.shinyapps.io/mriapp/>

# Segmentation

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# Segmented Brain



# How to achieve best segmentation

## Voxels intensity

Voxel brightness indicates tissue type (normalization is not easy though). Typically **Gaussian Mixture Model** is used.

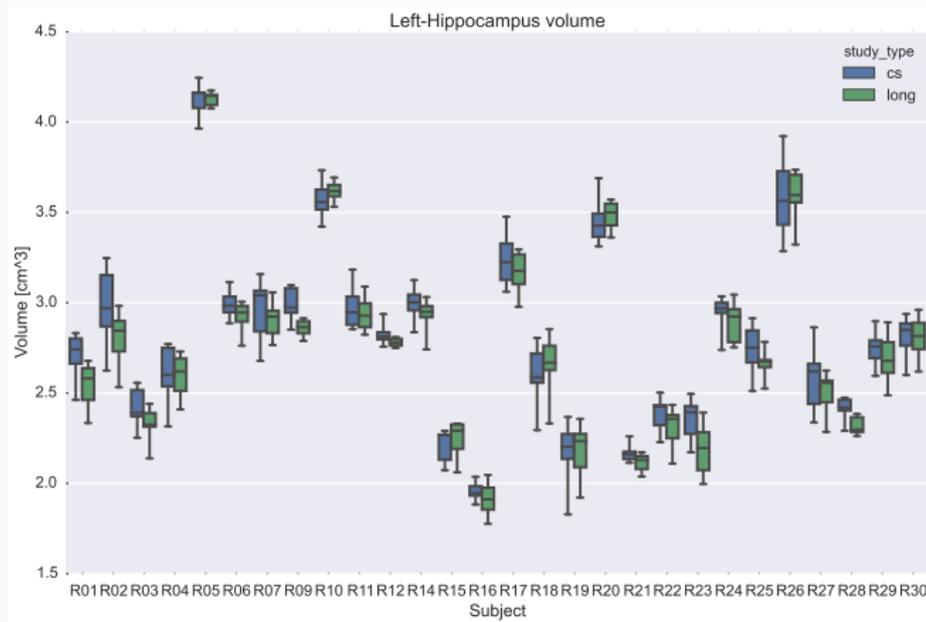
## Spatial coherence

*Voxels belonging to the same tissue will be likely next to each other.*  
**Markov Random Fields** could be used to force coherence.

## Apriori information

We approximately know where to look for hippocampus (and other ROIs). Take brains that have been already labeled, deform our brain onto them and construct **probabilistic map** that is used as an apriori probability (in a Bayesian sense). Even better is to use other scans of the same person from the longitudinal study → **longitudinal segmentation**.

# Effect of Longitudinal Segmentation on Volume Measurements



Error reduction from 3.54% to 2.50%

Detailed view <https://multi-armed-bandit.shinyapps.io/mriapp/>

# Atrophy Measurements

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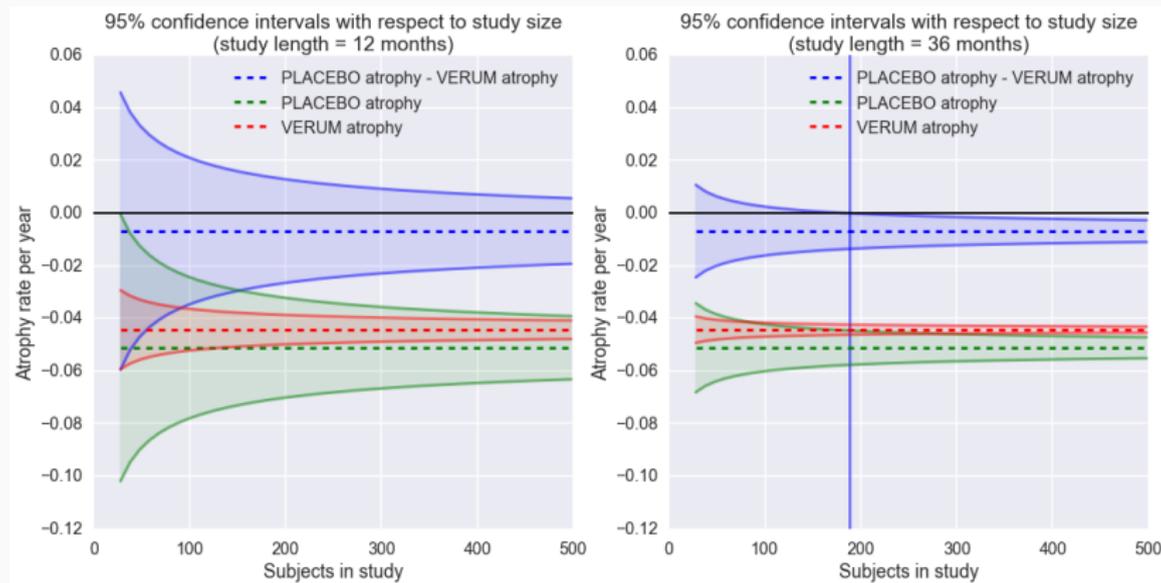
# Atrophy Measurements

$$\log(\text{volume}) \sim \text{time} : \text{Treatment} + (1 + \text{time} | \text{subject})$$

	Coef. FE			Std.Err. FE			loglike
	Intercept	time:Tr[PLACEBO]	time:Tr[VERUM]	Intercept	time:Tr[PLACEBO]	time:Tr[VERUM]	
Left-Hippocampus	7.952	-0.051	-0.047	0.033	0.010	0.006	314.213
Right-Hippocampus	8.005	-0.049	-0.048	0.039	0.012	0.007	310.510
Left-Cerebellum-White-Matter	9.544	-0.039	0.004	0.036	0.019	0.012	167.157
Right-Cerebellum-White-Matter	9.530	-0.032	-0.012	0.027	0.017	0.011	189.978
Left-Amygdala	6.946	-0.041	-0.060	0.050	0.022	0.013	155.173
Right-Amygdala	6.994	-0.052	-0.048	0.047	0.030	0.017	165.088
Left-Lateral-Ventricle	10.006	0.107	0.073	0.059	0.045	0.025	197.936
Right-Lateral-Ventricle	9.891	0.104	0.076	0.061	0.039	0.022	215.307
lhCortexVol	12.033	-0.052	-0.047	0.023	0.012	0.007	316.225
rhCortexVol	12.057	-0.048	-0.035	0.026	0.013	0.008	326.390
CortexVol	12.739	-0.051	-0.041	0.024	0.012	0.007	328.307
CorticalWhiteMatterVol	13.027	0.014	0.010	0.025	0.012	0.007	322.764
TotalGrayVol	13.086	-0.037	-0.032	0.018	0.009	0.005	358.729

# Sample size estimation

Length of study in longitudinal studies is more important<sup>2</sup> to significance than number of subjects.



<sup>1</sup>Assuming linearity of atrophy

# Preliminary Results

- Not enough samples to make any statistically valid conclusions
- Need to wait for more patients from Phase II and Phase III or additional scans from current patients
- Our primary aim right now is to **reduce measurement error** and set up **infrastructure for data processing**

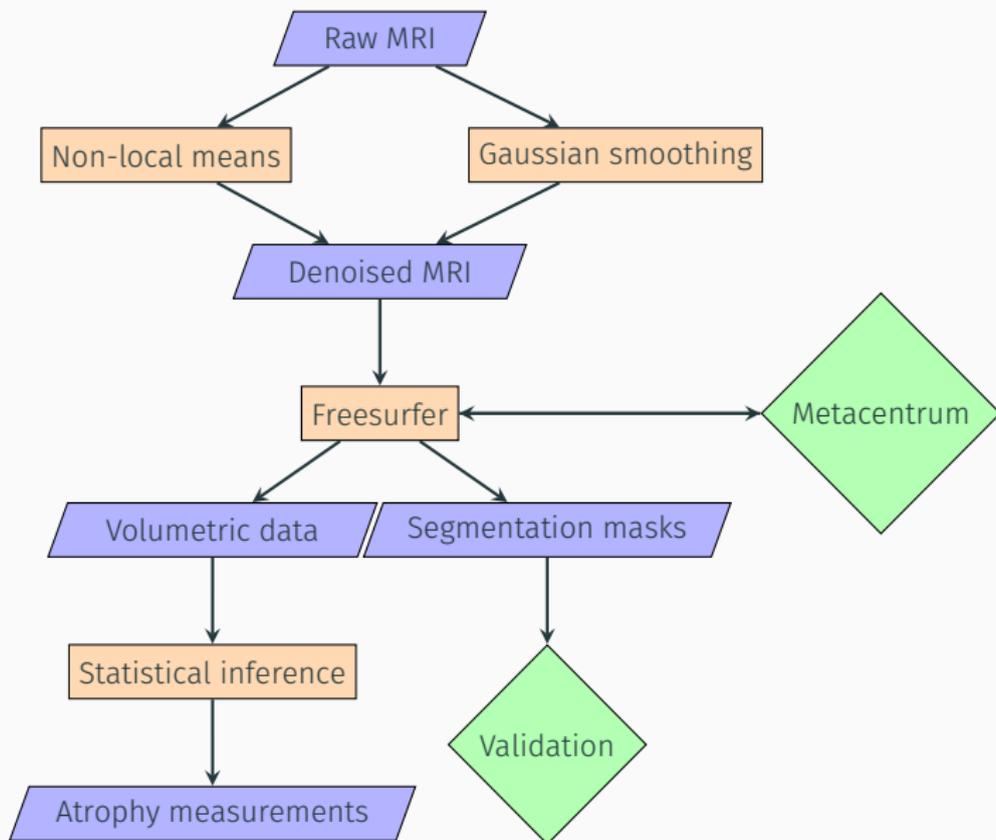
# Practical Considerations

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# Computation

- 28 patients x 5 scans x 3 methods x 6 hours = 105 days of processing time
- We utilized MetaCentrum clusters
  - Access to almost infinite computational resources
  - Easy to get started, setup scripts were really simple
  - Reduced processing time to 6 hours due to parallelization
- Other software claim to be faster than Freesurfer, but had other issues
  - Not an end-to-end analysis like Freesurfer
  - Need for parameter tuning
  - Closed-source
  - Lack of command line interface or API (only application was available)

# Processing Pipeline



## Future Work

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1. Upcoming Freesurfer 6.0 release implements **hippocampal subfields** segmentation that combines T1 and T2 scans to improve segmentation accuracy.
2. **Phase II** of clinical trial
3. Using **neural networks** for denoising (work in progress, not very promising so far)

Thank you for your attention!

Questions?

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